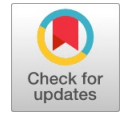


Automatic Eye Screening Method Based on a Multi-Anatomical Retinal System Segmentation with the Help of Morphology & Fuzzy Logic

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ABSTRACT: Eye examination is used to determine Retinal problems at an early stage. Retina screening can be used to detect various hidden retinal problems including pre-diabetes and diabetes. The doctors will depend on segmentation results of retinal structures to determine the abnormalities in the eye. A novel algorithm for instant identification and segmentation of the optic disk (OD) and detection of exudates in human retinal images is described in this document. The proposed technique uses segmentation methodology for automatically detecting of these structures. This methodology uses morphology theories and fuzzy techniques to detect the structures even in pathological images. The performance is evaluated using two datasets that is DRISHI-GS (optic disc) and DIARET1 (exudates). Present methods have accuracy and efficiency is less, but in the proposed new novel method i.e morphology based fuzzy logic, we achieved an accuracy 92.91% and PPV (positive predictive value) is 89.54% in optic disc. specificity and F-score also trained with help of subjected method 99% and 93.17% in exudate .

KEYWORDS: Retinal structures, optic disc, exudates, morphological theory, fuzzy logic, fuzzy c-means, convex hull transform.

INTRODUCTION:

Despite of the fact that the retina lives in a fringe area, it has some portion of the focal sensory system, speaking to bit of the neural eye [1]. The morphological diversity in retinal anatomical systems provides an exceptional indicative motivation as it includes important information for identifying as well as analysing a retinal pathology variation. One of the significant sickness that can hit the strength of eye in all is the diabetes. Diabetic nephropathy between many working-age people is one of the most well-known triggers of sight misfortune. Approximately 50% of instances of sensory impairment can be prevented by premature summary and occasionally by retinal testing. In beginning times of diabetic retinopathy, no extreme manifestations can be noticed, be that as it may, over the time, numerous manifestations start to show up and its seriousness expanded religiously through instant [4]. Normally, diabetic retinopathy method starts as a small adjust in retinal veins; in this way, the first variation from the normality container be distinguished is the presence of Microaneurysms. At that point, it influences the optic circle (optic nerve head) prompting variations in the optic circle outline.

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On the off chance that retinopathy is identified sufficiently early, treatment can stop it deteriorating. Something else, indications become perceptible with time, moreover, it is more difficult to treat [2].

RELATED WORK:

Sangita Bharkad[9] exhibited a calculation which depends on equiripple lowpass FIR channel and morphological tasks for programmed identification of OD focus, OD area and OD edge. Diabetic nephropathy between many working-age people is one of the most well-known triggers of sight misfortune. Approximately 50% of instances of sensory impairment can be prevented by untimely summary and occasionally by retinal testing. Carmen Alina Lupascu[10] commitment displays a robotized technique to find the optic circle in shading fundus pictures. The technique employments surface descriptors and a relapse based technique all together to decide the best circle that fits the optic plate. An assessment of the proposed technique has been done utilizing a database of 40 pictures. On this informational collection, our technique made 95% progress rate for the restriction of the optic circle and 70% achievement rate for the recognizable proof of the optic plate form (as a circle). AkaraSopharak [11] suggested a programmed scheme for recognizing exudates from small-contrast computer-controlled images of individuals with retinopathy, using a bunching method of Fuzzy C Means (FCM). Difference upgrade pre-processing is connected prior to four highlights, to be specific force, standard deviation on power, Tone and different border pixels are divided to provide fine separation input dimensions using FCM wrinkling method. The main outcome with morphological schemes is then calibrated. M. MoazamFraza[12] showed a bootstrapped decision groves design classifier for multi-scale limitation and exudate separation in retinal fundus images. At good grain and coarse grain concentrations, the candidate exudates are segregated using morphological development and specific Gabor canal. The appropriate indications are linked to the favourable exudates, which considerably decreases the exudate division's fake starting scores. A few area-based images are handled to plan the meeting classifier for pixel exchange as an exudate and non-exudate district from promising fields.



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The main drawback of these works is, it detects only one disease or structure and another disadvantage is that it depends on other works for segmentation of target structure. The main goal of this paper is it detects more than one result by using the same algorithm which focuses on reducing of computation task and time.

PROPOSED SYSTEM:

The proposed algorithm uses morphology theory and fuzzy c-means algorithm for detecting also segmentation of optic disc and exudates. For segmentation of these structures region wise Thresholding technique is utilized. This algorithm comprises of 3phases. The first stage aims in finding of ROI, second stage aims in coarse segmentation and third step aims in soft segmentation. The result of segmentation structures is shown below in the crystal format. The system algorithm uses same methodologies to segment these two structures.

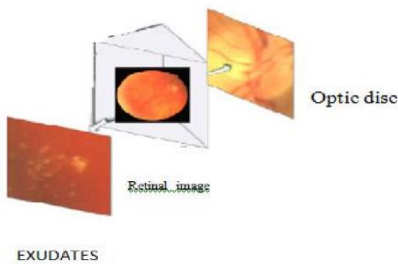


Figure1: Crystal of Segmentation structures

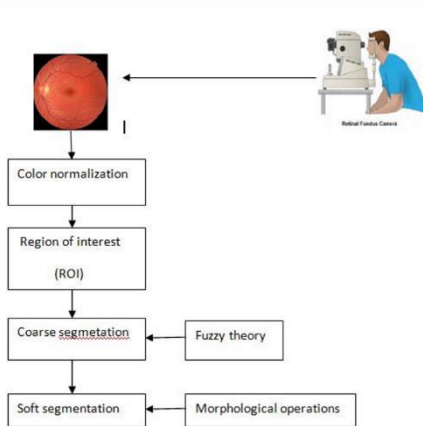


Figure 2 : Flow chart of proposed system

The flowchart of the proposed system is shown in fig 2. It contains of three steps finding the ROI is the first step, second step is coarse segmentation and last step is soft segmentation. Fuzzy theory is used in second step and morphological operations is followed by convex hull transform is used in last step.

OPTIC DISC:

STEP 1: The major idea of this step is to find ROI that is, to find the area of optic nerve head, square window around the region is obtained.

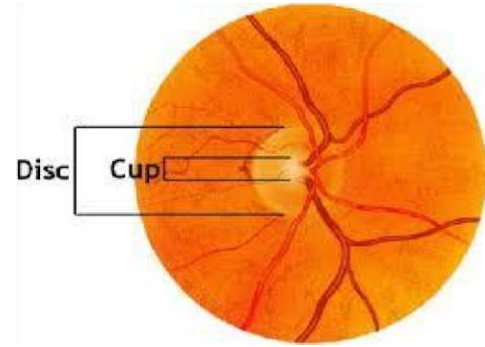


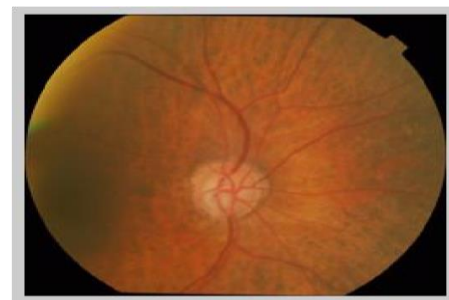
FIGURE3: Optic disk

Optic disc is almost round in shape, so we go for Hough transform. Edge map will be the first step to this. The performance will be increased by perfectly selecting the center for that fuzzy c means clustering is adopted. The first process is to extract red layer from the color image by using the below equation.

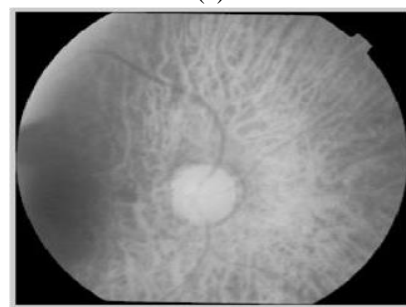
$$I_{R \text{ retina}} = \lambda R (I_{RGB \text{ retina}}) \lambda R(.) \quad (1)$$

Eq1 indicates the red layer extraction. opticnerve head can be seen clearly in the red layer than the remaining structures. To increase the visual color of the image CLAHE operator is utilized. $I_{\text{enhanced retina}} = \lambda \text{CLAHE} (I_{R \text{ retina}}) \lambda \text{CLAHE} (.) \quad (2)$

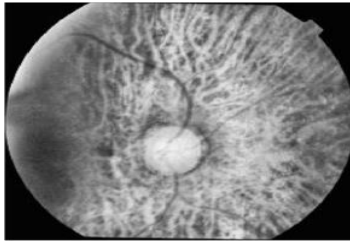
indicates the CLAHE operator. Median filter is used to increase the enhancement and is applied to FCM algorithm.



(a)



(b)



(c)

**Figure4: (a) color image(b)red layer
(c)CLAHE operator.**

As an initial move en route for edge map extraction is to spread on an 25-bunches FCM calculation on separated I improved retina picture through a objective of generally combining OD pixels hooked on one bunch also the other 24 bunches were devoted aimed at additional encompassing tissues. This task yields a 25-dim scaled picture IFCM

$$I_{FCM}^{bw} = \begin{cases} 1, & IFCM=C \\ 0, & OTHERWISE \end{cases} \quad (3)$$

I_{FCM}^{bw} indicates gray image where $c=25$ bunches. The targeted edge map consists of noises and other residues to remove this we go for morphological dilation operation. Then we go for Hough transform with resultant edge maps.

HOUGH TECHNIQUE:

It is that in the focal region of the table the reverse rows to the top function of a triangle bend (harmonize). Therefore, if we are unlikely to write reverse rows to each border pixel of our border chart, at that point districts of circles focuses will show up as splendid 'problem area' because of aggregate opposite lines there. Hough technique can be determined utilizing various methodologies: Directional data (paths), blunder charge (mapping) and variable room placing of a vote. Because we only have one lens tray for each image of the retina fundus, our circle-looking problem is reduced to one ring. We are using the last methodology in this manner. Parametric room placing a vote strategy remains as it is pursued: optic tray can be described as a ring-moulded object in the y and z fund screen image para as indicated metrically as

$$(x-a)^2 + (y-b)^2 = r^2 \quad (4)$$

Where a and b are the instructions of the promising ring concentrate, the optical panel matrix is concerned, and r is the radius. Although shift is a path to alter curve, nervous pixels (forces at (x, y) pixel) are linked in order to create a loop curve. The image focus given by the edge finder is regarded to be focused on the curve of the searched after the specified curve. For each edge pixel .x; y/, a competitor hover of $r \in [R \min; R \max]$ can be defined in

$$a = r \cdot \sin(\theta) \quad \forall \theta \in [0, 2\pi] \quad (5)$$

$$b = r \cdot \cos(\theta) \quad \forall \theta \in [0, 2\pi] \quad (6)$$

recognizing circle bend that best edge focuses continues through dening a gatherer exhibit

$$a = (r \cdot \sin(\theta)) + 1 \quad (7)$$

In our job, we separately speculated R min and R max at 75 and 85 pixels lengthy; this spectrum refers to the radii scope of promising models that are regarded in the search for OD ring. This range may fluctuate from one dataset to another depending on the objectives of the fundus picture, as it is compatible with the one dataset due to the standardized nature of the area as well as size of the optical circle. For each border pixel x; y / in Cartesian x y plane of the retina fundus image, a ring curve produced in linear ($r \wedge$, any) room. Applicant produced hovers converge in pinnacles (Or;) in Hough change space. Thus, places with greater splendor (collecting people) should be discovered in places where circle center should be discovered. Since we have one ring, one issue area is related to the OD region ($\max(A(r \wedge))$).

C: OD_ROI WINDOWPANE

Since Hough change identifies the directions (x_{center} ; y_{center}) of optical plate circle, an ideal circle canister be combined given a span r. Picking sweep esteem relies upon the approval dataset utilized; in light of the fact that each dataset created by means of fundus camera is of specific specifications regarding picture measure and pixel goals. Range esteem r was utilized in our framework to build up the square widows' fringes of optic plate district as it rises to 2.r pixels width. At that point, utilizing MATLAB picture trimming capacity final I_{ROI}^{OD} is obtained.

STEP2: SEGMENTATION:

This step uses the fuzzy theory to segment the targeted_ structure. Firstly intensity values of image are converted into membership values by properly selecting membership function. Each output of the step1 is considered as an one fuzzy set and each set consists of large no. of zones. All the zones consists of targeted structures only one zone will be the background. Fuzzy c-means are used for conversion of these values into clusters. FCM grouping is a covering grouping calculation, where each point may have a place with two or more groups with various degrees of participation. If the attributes of an image is same, then they are grouped into same class. The likeness of the class can be defined as distance of the attributes vectors to the group center most. Euclidean separation is utilized to gauge this separation and information will be related to a suitable participation esteem [24, 29, 30].



Automatic Eye Screening Method Based on a Multi-Anatomical Retinal System Segmentation with the Help of Morphology & Fuzzy Logic

The team attention is upgraded until the nearby goal job comparison, as shown in Equation is close to null or literally not precisely a predefined little coherent:

$$J_m = \sum_{i=1}^M \sum_{j=1}^C u_{ij}^m \|x_i - c_j\|^2 \quad (8)$$

Where m is an exponential weighting capacity which controls the fluidity of the registration work, the number of highlights is set to $2.M$. C is a group amount. u_{ij} is the enrollment level of x_i in bunch j , x_i is the dimensionally estimated information i th, c_j is the bunch's measuring focus, and is any standard that communicates the similarity between every deliberate element and the inside. Fluffy parceling is carried out by an iterative streamlining of the goal job shown above, with the u_{ij} registration extension and Equations ' lot targets c_j .

$$u_{ij} = \frac{1}{\sum_{k=1}^C \left(\frac{\|x_i - c_j\|}{\|x_i - c_k\|} \right)^{\frac{2}{m-1}}} \quad (9)$$

$$c_j = \frac{\sum_{i=1}^M u_{ij} x_i}{\sum_{i=1}^M u_{ij}} \quad (10)$$

The repetition will stop when below equation is fulfilled.

$$\text{Max}_{ij} \{ |u_{ij}^{(k+1)} - u_{ij}^{(k)}| \} < \epsilon \quad (11)$$

where ϵ is an end rule, 0.00001 for our case. k is the cycle number, it is set to a limit of 200 for our case. This system joins to a neighbourhood least or a seat purpose of J_m . The contribution to the FCM calculation is a lot of highlights. Rhe calculation is made out of the accompanying steps:

Stage 1: Initialize the fuzzy segment grid

$U = [u_{ij}]$ ($U(0)$) (12) by creating irregular numbers in the run 0 to 1 subject to Equation

$$\sum_{i=1}^M \sum_{j=1}^C u_{ij} = 1 \quad (13)$$

Stage 2: At k -step: compute the focuses vectors

$$C(K) = [c_j] \quad (14) \text{ with } U(K) \text{ as per the above}$$

Equation Stage 3: Update the fluffy segment grid $U(K)$, $U(K+1)$ by the new processed u_{ij} as indicated by Condition 2.

Stage 4: Compute the target work as indicated by the Equation. On the off chance that the distinction between neighbouring estimations of the target work is not as much as end basis (ϵ) at that point stop the emphasis; generally come back to stage 2. The yield from FCM grouping is a rundown of bunch focuses and n enrollment grades for every pixel, where n is various wanted bunches. A pixel will be relegated to the group with most astounding enrollment grade.



Figure5: FCM output of optic disc

STAGE 3:

SOFT SEGMENTATION:

The main goal of this segmentation is to get smooth output. The output of fcm consists of some noise and un necessary residues. so, we go for morphology dilation and opening operations. In order to get perfect shape for optic disc, we go for convex hull transform. This transform adjust all the points in order to get perfect shape of the structure.

PERFORMANCE EVALUTION

The performance is evaluated by using the formulas

$$\text{Sensitivity} = TP / (TP + FN)$$

$$\text{Specificity} = TN / (TN + FP)$$

$$\text{Accuracy} = (TN + TP) / \text{TOTAL}$$

$$\text{Precision} = TP / FP$$

$$\text{F-score} = TP + PPV / 2$$

RESULTS:

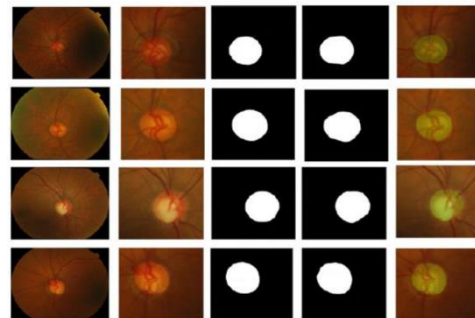


Figure6: Results of optical segmentation of the DRISHTI-DS dataset. Column 1: original retinal pictures. Column 2: Interest region. Column 3: The truths of the surface correspond. Column 4: Results of our suggested scheme for optical disk segmentation. Column 5: Overlapping.

TABLE1: Comparison of various optic nerve head segmentation results.

Method	sensitivity	specificity	PPV(positive predictive value)
Bharkad et al. (2017) [9]	74.60%	99.6%	74.96%
Kande et al.(2008)[13]	88.08%	98.78%	54.48%
Lupascu et ai.(2008)[14]	68.48%	99.69%	81.17%
Proposed Method	99.38%	99%	92.40%

TABLE2: optic nerve head performance comparison results based on DRISHTI-GS dataset

Method	F-Score
Wong et al. (2008) [15]	91.1%

Cheng et al. (2013) [7]	92.1%
Proposed Method	93.17%

The proposed method had segmented the optic disc and have succeed the highest performance in terms of sensitivity, specificity, precision and f-score. Optic disc segmentation is authenticated by exhausting the DRISHTTI-GS dataset. In medical usage if we can adopt this methodology to facilitate the doctors to easily segment optic disc with more accuracy. So, that doctors can detect glaucoma from the patient's retinal images.

EXUDATES

STEP 1: The existence of exudate fields is 1 of the true pointer of the proximity of diabetic retinopathy. Fig. 11.A shows a visit of a shading retinal fundus situation for a person who has transmitted various exudate fields alongside pixel tier remarks produced by retinal anatomical segment constructions. The extraction of exudate locale of intrigue pursues a similar technique utilized in optic circle extraction. Be that as it may, the district of the optic plate is supplanted with dark locale; in this way, exudate islands can't be misclassified as the optic circle district amid division stage, as appeared in Fig. 9.b.

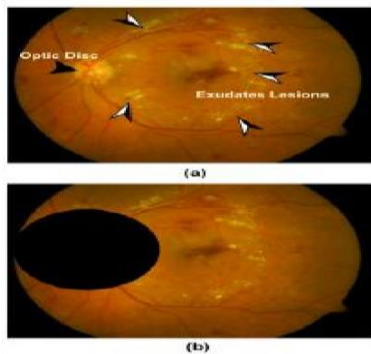


FIG 7: (A) Color Retinal Image (B) ROI Exudate.

STEP2: SEGMENTATION

The segmentation of exudate region follows the same procedure as that of the optic nerve head instead red region is replaced by black region.



Figure8: FCM output of exudate.

STEP 3: SOFT SEGMENTATION

The output of the fcm consists of the some of misclassified as a result we go for morphological dilation followed by opening. To get

perfect shape we go for same convex hull transform used in optic nerve head.

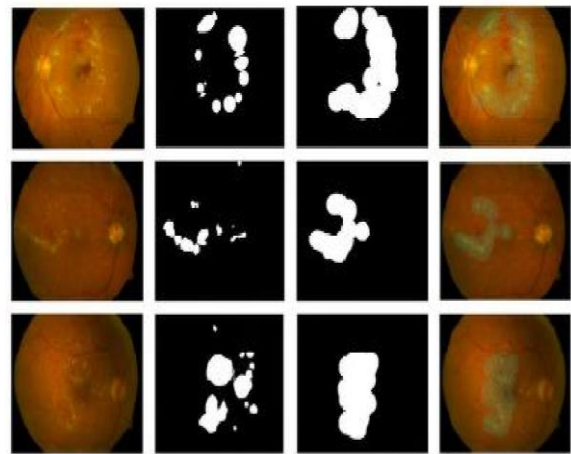


FIGURE9. Normal example of retinal exudates sores division results utilizing DiaRetDB1 dataset
Column 1: Original retinal pictures.
Column2: Relating ground realities. Column 3: Exudates injuries division after effects of our proposed framework.
Column 4: Superimposed division results.

TABLE3: Performance comparison results of exudates using DiaretDB1dataset in pathological images.

Method	Sensitivity	Specificity
Welfer et al. (2010)[17]	70.48%	98.64%
Liu et al. (2017)[16]	83%	75%
Proposed Method	89.76%	86.72%

Method	Accuracy	PPV
Liu et al. (2017)[16]	79%	
Fraz et al. (2017)[12]	87.72%	87.14%
Proposed Method	92.91%	89.54%

As appeared in Fig. 9.a, exudate sores show up as either white or yellow delicate irregular areas of various sizes, non uniform shapes and fluffy disparity on the surface of retinal fundus pictures. In spite of the fact that retina exudates pursue neither uniform estimating nor a uniform power circulation, the optic nerve head and splendid reflections inside void retinal vessels show a



Automatic Eye Screening Method Based on a Multi-Anatomical Retinal System Segmentation with the Help of Morphology & Fuzzy Logic

comparable appearance. The exudate injuries speak to both

CONCLUSION:

The proposed methodology is helpful inside detecting and segmenting of exudates. The investigated method is evaluated with the active methods. Our proposed methodology is checked with the DiaRetDB1 dataset. The performance analysis of the proposed method had achieved high in every parameter when compared it with the existing methodologies.

The proposed methodology had detected and segmented the optic disc and exudates in one session by using morphology and fuzzy theory. For medical perceptible the separation of structures is the first stage in the scheme for further improvement of PC related helped analytic frameworks for ophthalmic issues.

The test results proved that the proposed methodology had achieved better results in all parameters such as sensitivity, specificity and accuracy for the similar dataset used. The proposed methodology is robust even if we have utilized the morphology and fuzzy theory. This will be the replacement to the crisp world to fuzzy one.

FUTURE WORK:

The future work of this proposed system can be focussed on segmentation of other retinal structures or organs can be concentrated. The future work will be focused on the two offerings. First there is no need of separate algorithms to segment one issue. The proposed system provides same methodologies for segmentation of more than one structure. Second this algorithm is very power because the performance is high even when it is compared it with other recent methods.

So, for clinical view it is very helpful in detecting more than one structure by using same algorithm.

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