

A Hybrid Pain Detection Technique using SVM Parameter Optimization and Contourlet-Gabor Transform Feature Fusion



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Abstract—This paper highlights automatic pain expression recognition from facial images of pain. This technique is frequently used in healthcare applications. The research detects the pain expression by an effective recognition method. It is based on the concepts of fusion of contourlet transform with Gabor transform for feature extraction, and classification of expressions by using SVM. The ABC algorithm and GA is implemented for optimizing SVM parameters. In order to authenticate the precision and stoutness of the system, a number of experiments have been done on two databases namely UNBC shoulder pain database and IFD-CEERI database. It's provided throughout the simulation techniques. The suggested strategy is actually effective in recognition of pain expression in terms of accuracy.

Keywords: ABC-SVM, GA-SVM, Face detection, Contourlet transform, Pain detection, Gabor filter

I. INTRODUCTION

The automated recognition of facial expression remains as one of the difficult task in the area of highly effective computing hitherto. Certainly, facial expression [1-3] is referred as the largely important, instinctive, and instantaneous method accepted by humans to communicate, express and exchange intentions, emotions, and thoughts. The physical or mental sickness of a person is best expressed in terminology of pain expression. It's extremely hard to create a reliable assessment of pain and after that organize the same in a clinical environment. Among the most broadly used methods is actually patient self report to measure up pain. The reason: it's ideal. It neither calls for switching to complex technology, neither does it necessitate any outstanding skills. Nevertheless, self report is actually self limiting and can't be used on substantial set of populations, like young children that are young, people with limited mental capabilities, patients facing issues in communication and speech, and those that need assisted breathing. Numerous researchers [4,5] have attempted in the past to deal with these shortcomings and attain a continuous unbiased assessment of pain using investigative approaches.

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Nevertheless, the above mentioned procedures have mostly been dragged down owing to the point that, frequently they're not found congruent with alternative verifications of pain, besides being extremely invasive and constricting to the patient.

Alternatively, a possible approach can be using facial actions to code pain, nearly equivalent to the "faces of pain" approach. Many features have been drawn from faces such as FACS [6-8], PCA [9, 10], AAM model [11, 12] and Gabor wavelet. Today, Countless methods have been applied to recognize pain. Majority of the prevalent automated facial appearance detection techniques largely rely on two important measures: facial characteristic withdrawal and categorization. However, the categorization result mainly depends on facial characteristic removal techniques, which should reflect human insight about images.

This work has proposed two new hybrid facial expression recognition approaches. These are the fusion of contourlet (CT) and Gabor transformation for feature extraction and classification of pain by ABC-SVM [13, 14] and GA-SVM [15]. Minh N. Dow and Wetterly [16] invented the contourlet transform, a 2-dimensional transformation method for image representation. The CT is stimulated by the human visual method and the Curvelet make over, which can take into custody different stretched shapes and smoothness of the contour of images in different directions. The SVM kernel- parameter optimization has been done using ABC [18] and GA separately to improve the accuracy of recognition. In order to recognize pain expressions of facial images taken from the various expression data base, the anticipated concept is employed to get precise and meaningful results.

The organization of the paper is as follows: Section 2 consists of brief discussion about the CT and Gabor transform. The section 3 describes with the proposed method and Section 4 represents the experimental result. Section 5 represents the brief conclusion of the research.

II. CONTOURLET AND GABOR TRANSFORM

2.1 Contourlet Transform

Do MN and Vetterli M. Contourlets, [17] introduced CT a directional multi resolution image representation program that has anisotropy and directionality, by virtue of its capability to represent smooth contours in a number of directions of an impression.



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In this particular channel bank (Figure 1), initially, the Laplacian Pyramid (LP) can be put to use to determine the point dissection of the picture succeeding the directional filter bank (DFB) in straight structures. In order to add anomalies, the above program comes about an image development which utilizes essential components as form servings, and appropriately it's termed as contourlet transform.

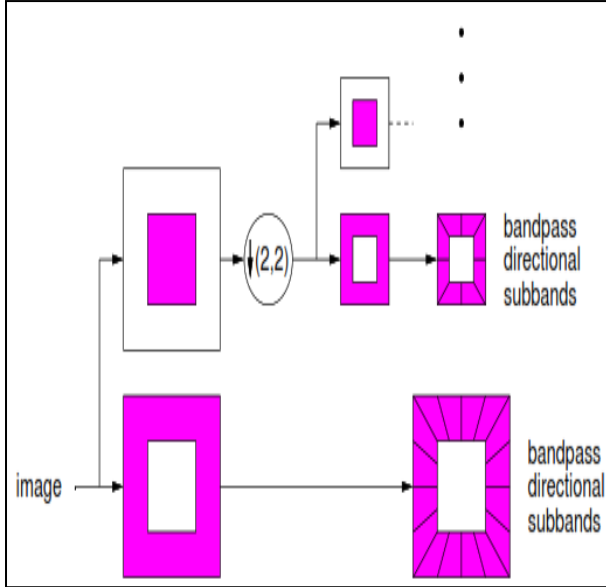


Figure 1: The contourlet filter bank

In the following part, we are going to discuss Multi resolution analysis which is even more categorised into the following categories:

2.1.1 Multi-scale

This refers to a multi-resolution analysis for the LP, like the one for wavelets. It's assumed that orthogonal screens had been used for the LP in the contourlet filter bank with down sampling by two in each dimension (which results in $N = \text{diagonalmatrix}(2,2) = \begin{bmatrix} 2 & 0 \\ 0 & 2 \end{bmatrix}$ as appeared in Figure2).

Under particular regularity circumstances, unique scaling function $\phi(t) \in L_2(\mathbb{R}^2)$ satisfy the equation (1):

$$\sqrt{2}\phi(t) = 2 \sum_{n \in \mathbb{Z}^2} g[n]\phi(2t - n) \quad (1)$$

For the low-pass synthesis filter Q, the impulse response is $q[n]$. Let

$$\phi_{i,n} = 2^{-i}\phi\left(\frac{t-2^i n}{2^i}\right), i \in \mathbb{Z}, n \in \mathbb{Z}^2 \quad (2)$$

At that point the family $\{\phi_{i,n}\}_{n \in \mathbb{Z}^2}$ is an ortho-normal cause for an approximation sub-space U_i at the range 2^i . Furthermore, $\{U_i\}_{i \in \mathbb{Z}}$ provides a preparation of multi resolution established subspaces where $U_2 \subset U_1 \subset U_0 \subset U_{-1} \subset U_{-2} \dots$ where U_i is linked with a uniform grid of intervals $2^i \times 2^i$, through that the image approximation will be completed at a scale of 2^i . Therefore, the difference images exists in a sub-space X_i which is the orthogonal counterpart of U_i in U_{i-1} , or $U_{i-1} = U_i \oplus X_i$

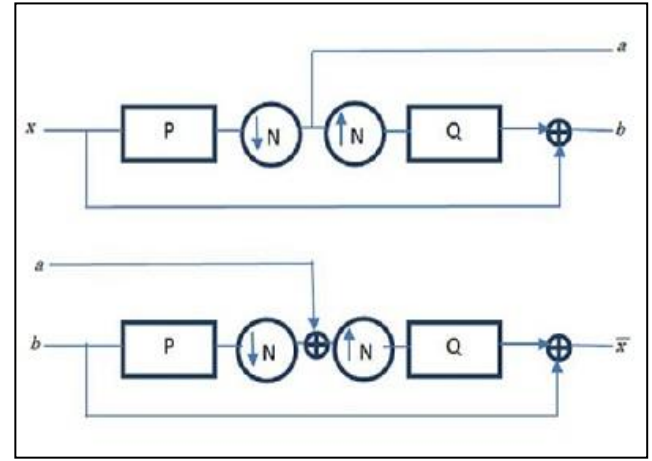


Figure 2: Laplacian Pyramid Method

It is understood [framing pyramids] that $b[n]$ with $a[n]$ in Figure2 begins from a separate filter bank channel with the similar sampling matrix $N = \text{diagonalmatrix}(2,2)$. $\Psi^{(j)}(t)$ is described as below:

$$\Psi^{(j)}(t) = 2 \sum_{n \in \mathbb{Z}^2} e_j[n]\phi(2t - n) \quad (3)$$

The impulse reaction of the high pass synthesis filter $E_j(Z)$ is $e_j[n]$. Now $\Psi^{(j)}(t)$ in eq.(3), would be $\Psi_{i,n}^{(j)}(t) = 2^{-i}\Psi^{(j)}\left(\frac{t-2^i n}{2^i}\right)$, $i \in \mathbb{Z}, n \in \mathbb{Z}^2$. Subsequently, for scale 2^i , $\{\Psi_{i,n}^{(j)}\}_{0 \leq j \leq 3, n \in \mathbb{Z}^2}$ is rigid frame for W_i . For all the scales, $\{\{\Psi_{i,n}^{(j)}\}_{i \in \mathbb{Z}, 0 \leq j \leq 3, n \in \mathbb{Z}^2}\}$ is a rigid frame for $L^2(\mathbb{R}^2)$. In the above mentioned cases, the frame bounds are nearby to 1. As W_i is generated by four kernel functions equivalent to multi-wavelets), commonly it is not a shift-invariant sub-space. However, a shift-invariant subspace is simulated by converting $\mu_{i,2n+f}(t) = \Psi_{i,n}^{(j)}(t)$, $0 \leq j \leq 3; f_i$ are the coset symbolize for down sampling by 2 in each dimension, i.e. $f_0 = (0,0)^T, f_1 = (1,0)^T, f_2 = (0,1)^T, f_3 = (1,1)^T$. Considering this characterization, the family $\{\mu_{i,n}\}_{n \in \mathbb{Z}^2}$ related to a uniform grid of intervals $2^{i-1} \times 2^{i-1}$ on \mathbb{R}^2 enlarges a rigid frame for W_i [17].

2.1.2 Multidirectional

By taking into account of multi-rate identities, as in Figure 3, the equivalent directional analysis filters are $E_k^{(l)}, 0 \leq k \leq 2^l$ and the directional synthesis filters are $D_k^{(l)}, 0 \leq k \leq 2^l$. Subsequently, the linked entire sampling matrix $S_k^{(l)}$ in the diagonal states is mentioned below.

$$S_k^{(i)} = \begin{cases} \text{diagonal}(2^{l-1}, 2), & \text{for } 0 \leq k < 2^{l-1} \\ \text{diagonal}(2, 2^{l-1}), & \text{for } 2^{l-1} \leq k < 2^l \end{cases} \quad (4)$$

$$\{d_k^{(l)}[n - S_k^{(l)}m]\}_{0 \leq k < 2^l, m \in \mathbb{Z}^2} \quad (5)$$

The design of the directional subspaces $W_{j,k}^{(l)}$ is produced by the usage of orthogonal filters in DFB executed on the difference image. The same has been shown in Figure 3:

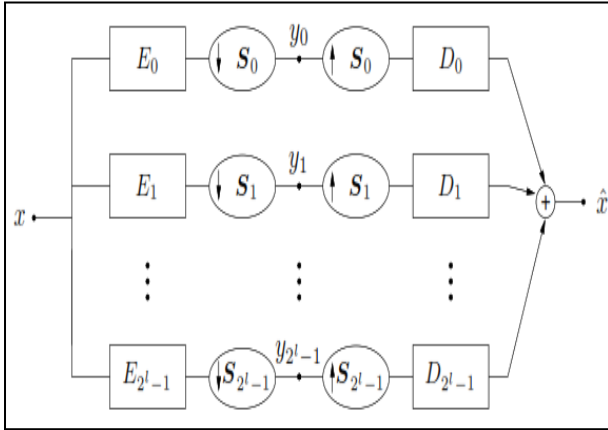


Figure 3: The multi-channel DFB

2.2 The Gabor filter method

In view of the fact that, feature extractions for facial recognitions through Gabor filters [20,21] provides good results, Gabor waveform oriented feature extraction method is executed here. The relation of two dimensional Gabor kernels is mentioned below.

$$W(x, y, \theta, \lambda, \phi, \sigma, \gamma) = \exp \left[-\frac{x'^2 + \gamma^2 y'^2}{2\sigma^2} \right] \cos \left[2\pi \frac{x'}{\lambda} + \phi \right]$$

$$x' = x \cos(\theta) + y \sin(\theta)$$

$$y' = x \sin(\theta) + y \cos(\theta) \quad (6)$$

In the equation 6 represents the location of a light impulse with standard notations.

Let $\mathbf{x} = [x' y']^T$ be the image coordinates.

Then, the impulse response of a Gabor filter $g(\mathbf{x})$ is to be expressed as given below:

$$g_{mn}(\mathbf{x}) = \frac{1}{2\pi a_n b_n} e^{-\frac{1}{2} \mathbf{x}^T A_{mn} \mathbf{x}} e^{j k_{0mn}^T \mathbf{x}} \quad (7)$$

Here, the matrix A represents the bandwidth and reference selection point of the filter.

$$A_{mn} = \begin{bmatrix} \cos \phi_m & -\sin \phi_m \\ \sin \phi_m & \cos \phi_m \end{bmatrix} \begin{bmatrix} a_n^{-2} & 0 \\ 0 & b_n^{-2} \end{bmatrix} \begin{bmatrix} \cos \phi_m & \sin \phi_m \\ -\sin \phi_m & \cos \phi_m \end{bmatrix} \quad (8)$$

If the direction of modulation frequency vector remains akin to that of one of the envelopes axes, with

$$k_{0mn} = k_{0n} \begin{bmatrix} \cos \phi_m \\ \sin \phi_m \end{bmatrix} \quad (9)$$

The transfer function G(k) of a Gabor filter is expressed by equation (10)

$$G_{mn}(k) = e^{-1/2(k-k_{0mn})^T (A_{mn}^{-1})^T (K-K_{0mn})} \quad (10)$$

where $k = [k_1 k_2]^T$ is the spatial frequency. If the expression of equation of modulation frequencies are given by equation (11)

$$k_{0n} = \frac{\pi}{2^{n+1}}; n \in [0 \dots N-1] \quad (11)$$

III. PROPOSED METHOD FOR PAIN RECOGNITION

The proposed technique has three key modules for pain expression recognition. They are:

- face recognition and image normalisation
- feature extraction and

- Expression Classification

3.1 Face Detection and image normalisation:

It's important to point out that Viola Jones visage recognition algorithm was applied for the item recognition as it provides the competitive face detection rates in real time. After completion of face detection, the necessary component was extracted using the cropping of the picture, therefore removing undesired component of the facial skin.

3.2 Feature Extraction

In the proposed technique of ours, we've extracted 2 sets of characteristics from the pictures, Figure 4, by working with contourlet transform and Gabor Filter as mentioned in subsequent sections.

3.2.1 Feature Extraction using Gabor Filter

The very first set of options, Fg, from the pictures had been extracted making use of the Gabor filters as per eq.(6). We're doing block averaging. Gabor filter highlights edges just in a particular direction and majority of picture has very low intensity. Then when we average blocks, blocks with no edges remains almost identical, whereas blocks with edges change the typical to greater intensity and that highlights particular features. Those characteristics are actually selected for the classification. Total 512 features, set one, were selected from the specified picture for the different parameters of Gabor filter as per equation (6)

3.2.2 Feature Extraction using CT

For feature extraction, set 2, F_{CT}, as denoted in Figure 3, In the changed domain, each pre-processed image is decoposed using the Contourlet transform to a level of 4. The majority related texture data is divided because of iterated low pass filtering, hence the data is possessed within the directional sub-band of the scale. It has been measured that the picture is dissected into 2¹ directions at 1st level, 2² at the 2nd level, 2³ at the 3rd level and 2⁴ at the 4th level. Therefore, we attain 30 i.e. (2¹+2²+2³+2⁴) directional sub bands for every image.

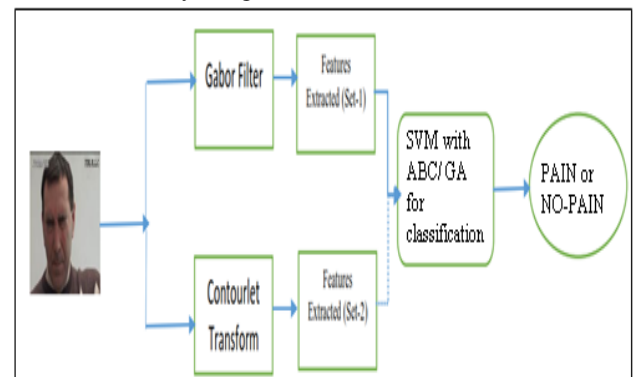


Figure 4: Feature Extracted using CT and Gabor filters fed to SVM for classification of pain

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Four levels of contour transformation are used to transform each facial expression as LP and DFB with the image PKVA filter.

Levels of 4, 3, 2 and 1 are raised in reverse order. The pre-processed image is decomposed in 24 directions at 1st level, 23 at 2nd level, 22 at 3rd level and 21 at 4th level. Total quantity of 30 i.e. $(2^4+2^3+2^2+2^1)$ directional sub-bands for each image are obtained. We extracted the set of features in FCT by calculating a 16 bin histogram for each sub-band. The total features 496 derived by means of CT are mentioned below (Figure 5):

$$\begin{aligned} F_{CT} &= [(2^4+2^3+2^2+2^1) \times 16 \text{ or } (2^1+2^2+2^3+2^4) \times 16] + [1 \times 16]; \\ &\text{with one feature for whole image} \\ &= [(30 \times 16) \text{ or } (30 \times 16)] + 16 \\ &= 496 \end{aligned}$$

The features, F_g & F_{CT} , were scaled down as mentioned below:

$$\begin{aligned} F_g &= (F_g - \min(F_g)) ./ (\max(F_g) - \min(F_g)) \quad (12) \\ F_{CT} &= (F_{CT} - \min(F_{CT})) ./ (\max(F_{CT}) - \min(F_{CT})) \quad (13) \end{aligned}$$

F_g & F_{CT} are joined together as mentioned below:

$$\text{The fusion function } F = \{F_g, F_{CT}\} \quad (14)$$

The total features extracted from the images, F , using these two methods, provided into the SVM classifier to classify the pain reactions.

3.3 Classification Techniques

After getting the features from the fusion of CT and GT, the classification techniques applied using SVM. Different kernels have been used and results were calculated with and without optimization of SVM parameters as mentioned in figure 5.

3.3.1 SVM without optimization

Support vector machines [19] are binary classifiers and has good ability to control and implement on high dimensional data and are wide-ranging taken into application for feature classification, believes a training data set $\{(x_1, y_1), (x_2, y_2), \dots, (x_n, y_n)\}$, where x_i are the vectorized training images and $y_i \in \{-1, +1\}$ are the labels to which each image can be allocated to.

SVM tries to create a hyper plane, $w^T z - b = 0$ which best divides the data points (by more difference) in which w is usual to the hyper plane and b is the prejudice and $\frac{b}{\|w\|}$ is the vertical distance between the hyper plane to the margin. The highest margin hyper-plane are traced by algorithm to calculate linearly divisible types. This will be done by minimizing the objective function of equation (15).

$$\begin{aligned} F(x) &= \frac{1}{2} w^T x \quad (15) \\ y_i(w^T x_i + b) &\geq 1 \quad \forall i \end{aligned}$$

For non-linear SVMs, sticking to the selected kernels, the Lagrangian is made the most of as shown below:

$$\begin{aligned} \max_a L_{Dual} &= \sum_{i=1}^l a_i - \frac{1}{2} \sum_{i,j=1}^l a_i a_j y_i y_j \langle x_i, x_j \rangle \\ \text{Subject to } 0 &\leq a_j \leq C \\ \sum_j a_j y_j &= 0 \end{aligned} \quad (16)$$

To calculate the optimal hyper-plane, a dual Lagrangian L_{Dual} should be maximized as per the nonnegative a_i mentioned as per the given parameters. To

calculate the optimal hyper-plane, a dual Lagrangian The penalty factor C is calculated by the user.

The Polynomial kernel is:

$$k(x_i, x_j) = (1 + x_i^T x_j)^P \quad (17)$$

$$\text{Gaussian (RBF) kernel: } k(x_i, x_j) = \exp\left(-\frac{\|x_i - x_j\|^2}{2\sigma^2}\right) \quad (18)$$

$$\begin{aligned} \text{Subject to } \alpha_i &\geq 0, i = 1, \dots, l, \\ \sum_{i=1}^l \alpha_i y_i &= 0, \end{aligned} \quad (19)$$

In Eq. (18), σ^2 denotes the variance of the Gaussian kernel.

3.3.2 Parameter Optimization of SVM using ABC and GA

SVM parameters can be optimized using various algorithms for classification of expressions. Here in this paper, we have used GA-SVM and ABC method to optimize the parameters as mentioned in the figure 5. We have considered linear, Gaussian and polynomial kernel.

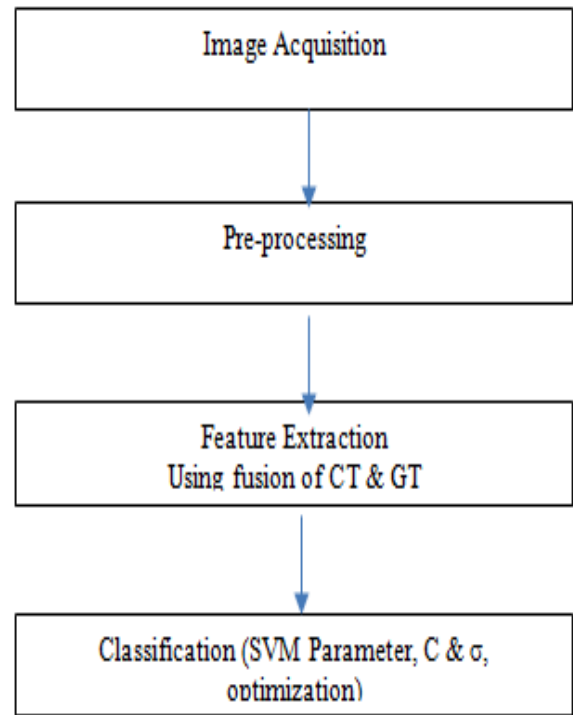


Figure 5: SVM parameter optimization

A brief description about the optimization techniques, which we have used, is given below:

A. The proposed GA-SVM model has SVM parameters which are animatedly optimized by putting into practice the RGA evolutionary process, as mentioned in figure 6, and the SVM model then performs the classification job by means of these optimal values.

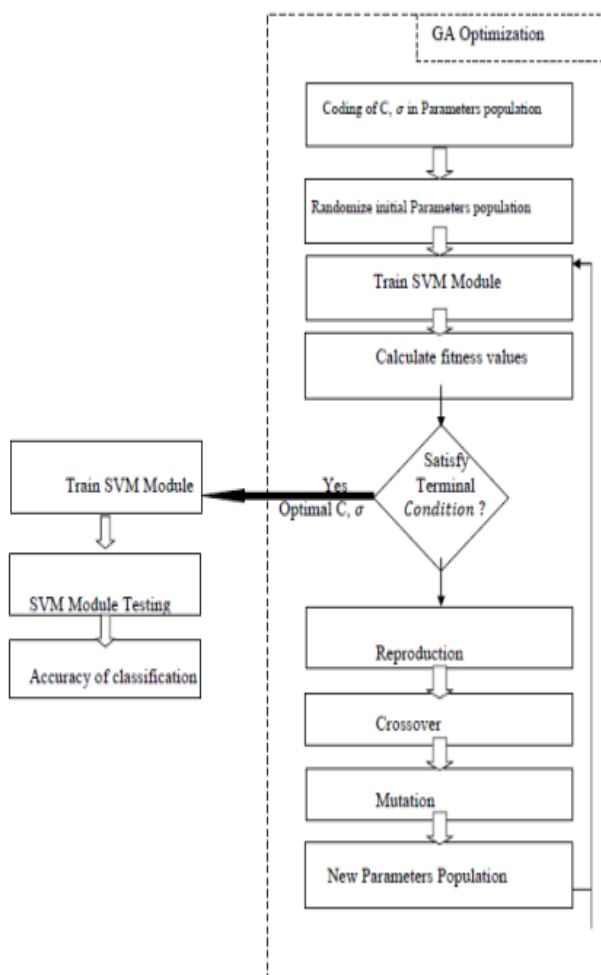


Figure 6: GA-SVM parameter optimization process

B. In ABC algorithm [18], the following three groups of the colony of artificial bees are there: engaged bees, observers and scouts. The initial 50% of the colony comprises the engaged simulated bees and the next half incorporates the observers. When we take into consideration each and every food resource, the finding is that we have only one engaged bee. We may also say that the overall engaged bees are equivalent to the total number of food resources in the region of the hive. Those engaged bee whose food supply have been discarded by the bees, the same gets converted into a scout.

In ABC algorithm, the arrangement of a food resource depicts a probable explanation to the optimization issues and the elixir quantity of a food resource matches up to the worth (fitness) of the connected clarification. The figure of the engaged bees or the observer bees is equivalent to the number of resolutions in the populace. At the initial move, the ABC creates an indiscriminately strewn preliminary populace $P(G)$.

A simulated observer bee prefers a food resource relying on the probability value linked with that food resource, p_i , designed by the following expression (20):

$$p_i = \frac{fit_i}{\sum_{n=1}^{SN} fit_n} \quad (20)$$

Where fit_i is the suitability value of the answer i which is comparative to the elixir amount of the food resource in the situation i and SN is the number of food resources which is equivalent to the number of engaged bees (BN).

$$v_{ij} = x_{ij} + \phi_{ij}(x_{ij} - x_{kj}) \quad (21)$$

where, $k \in \{1, 2, \dots, SN\}$ and $j \in \{1, 2, \dots, D\}$ are arbitrarily selected indexes. However, k is evaluated arbitrarily, it has to be dissimilar from i . ϕ_{ij} is an arbitrary number between $[-1, 1]$. It is in command of the creation of neighbour food resources roughly x_{ij} and symbolizes the relationship of two food locations optically by a bee.

Comprehensive Pseudo-code of the ABC algorithm is as follows:

1. Initializing the populace of answers x_{ij} , $i = 1, \dots, SN$, $j = 1, \dots, D$
2. Assess the populace
3. No of cycle = 1
4. Replicate
5. Create fresh explanation V_{ij} for the engaged bees by means of (21) and assess them
6. Apply the greedy choice process
7. Work out the probability values P_{ij} for the resolutions x_{ij} by (20)
8. Generate the fresh solutions V_{ij} for the observers from the solutions x_{ij} selected on the basis of p_{ij} and estimate them
9. Applying the greedy selection method
10. Establish the deserted solution for the scout, of exists, and substitute it with a fresh arbitrarily created solution x_{ij} .
11. Learn by heart the paramount solution accomplished hitherto
12. Cycle = Cycle + 1
13. In anticipation of cycle = MCN

IV. DATABASE FOR THE VERIFICATION

The proposed methodology is implemented on following two datasets:

4.1 UNBC Shoulder Pain Expression database, which acts as the base to verify the proposed algorithm, using MATLAB. It has the videos of the faces of 63 male, and 66 female with shoulder injuries as shown in figure 7. The image depicts the shoulder pain of the subjects in way of the transform of position, problematic and unproductive shoulders through active and passive circumstances. Subjects started their shoulder rotation by themselves in the active location.



Figure 7 : Examples of some of sequences from the - McMaster Shoulder Pain Expression Archive Database

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4.2 The Indian Face Database – CEERI (IFD-CEERI) has been built at the Perception and Cognition Engineering Lab in the IC Design Group of CEERI-Pilani. It has 259 persons (192 males and 67 females) in the age groups of 0-17, 18-29, 30-44, 45-64, and 65-90 years. The dimension of every picture is 720 x 576. For the verification of proposed algorithm, we have taken face images of pain from the database as shown in figure 8.



Figure 8: Examples of some of sequences from the - CEERI Expression Database

Table 1: Accuracy using SVM Classifier for levels (4, 3, 2, 1) with parameter optimization techniques (for UNBC shoulder pain database)

Expression	Recognition Accuracy (%)			Recognition Accuracy (%)			Recognition Accuracy (%)		
	Linear	Linear with GA	Linear with ABC	RBF	RBF with GA	RBF with ABC	Polynomial	Polynomial with GA	Polynomial with ABC
Pain	97.62	97.81	97.94	95.52	96.43	96.54	97.28	97.35	97.48
Non-Pain	99	99.23	99.35	100	100	100	100	100	100
Average	98.31	98.52	98.65	97.83	98.22	98.27	98.64	98.68	98.74

V. EXPERIMENTS AND RESULTS ANALYSIS

Here, after the pre-processing, as per the equation (14), the collective features were implemented to SVM for classification and a comparison was created among the classification accuracy achieved from optimization of SVM parameters using ABC and GA (Table 1 & Table 2). The results reported clearly denote that the collective features are producing good classification accuracy with ABC-SVM as compared to GA-SVM. SVM used here, categorizes Objects in two groups, hence classification is done by One-v/s-One and One-v/s-All both the techniques, which trains classifiers to create a distinction of one expression from another. Various kernels of SVM have various forces on pain recognition rate. We implemented three SVM kernels namely linear, Polynomial and RBF kernels.

The performance obtained through various kernels for shoulder pain database is tabulated in Table 1 for combined features, where CT levels used here are (4, 3, 2, 1) as we have better results for these levels [22]. There is an increase in accuracy of recognition when we have applied various parameter optimization techniques on SVM. Figure 9 shows a comparative analysis between various methods applied.

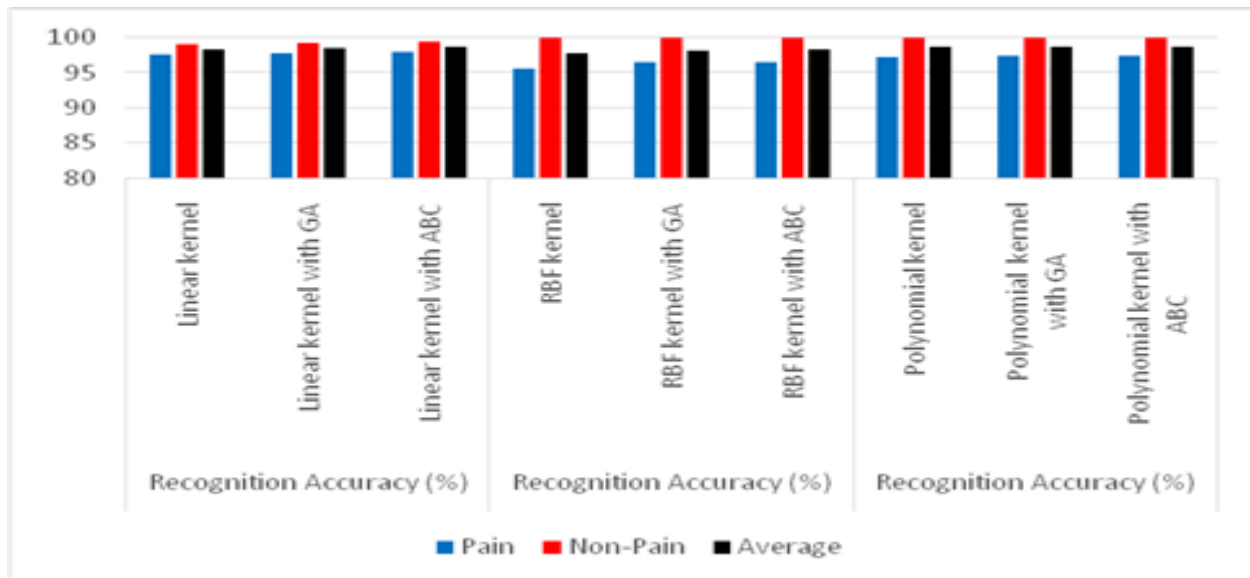


Figure 9: Comparison of accuracy achieved using various methods (UNBC Shoulder Pain Database)

We have also applied the proposed method on IFD- accuracy compared to other techniques as mentioned in CEERI database also and there also we have achieved better table 2 and figure 10.

Table 2: Accuracy using SVM Classifier for levels (4, 3, 2, 1) with parameter optimization techniques (IFD-CEERI Database)

Expression	Recognition Accuracy (%)			Recognition Accuracy (%)			Recognition Accuracy (%)		
	Linear	Linear with GA	Linear with ABC	RBF	RBF with GA	RBF with ABC	Polynomial	Polynomial with GA	Polynomial with ABC
Pain	96.64	97.23	97.57	95.54	96.05	96.36	96.56	97.22	97.49
Non-Pain	97.22	97.89	98.43	96.72	97.32	97.89	97.13	98.03	98.54
Average	96.93	97.56	98.00	96.13	96.69	97.13	96.85	97.63	98.02

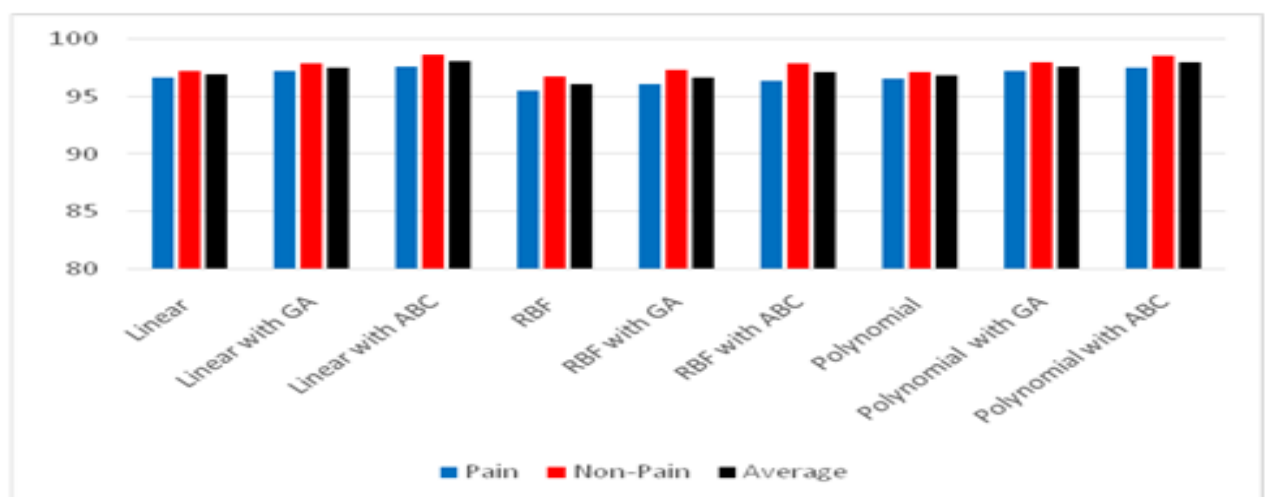


Figure 10: Comparison of accuracy achieved using various methods (IFD-CEERI Pain Database)

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We're getting much better outcomes by utilizing the suggested technique through the combined characteristics with polynomial kernel with ABC-SVM, which is also reported in Table 3 for shoulder pain database.

Table 3: Comparison of accuracy of our method with other methods

Method	Average Recognition Rate
AAM and SVM [8]	82% accuracy
AAM, SVM [7]	79.66% accuracy
AAM, Log-normal filters and SVM[23]	73% accuracy
DCT, LBP, RVR [24]	92% accuracy
Gabor, PCA,SVM [9]	95.5%
Fusion of CT with GT [22]	98.64%
Our Method, Fusion of CT with GT with SVM parameter optimization	98.74%

To optimize C and σ , we have applied two algorithms namely, Genetic algorithm and Artificial Bee Colony, ABC, algorithm. Therefore, the primary goal of these implementations is to apply these new models to increase the classification accuracy of pain expression recognition. The results obtained from ABC-SVM model are even better than GA-SVM. There is an increase in accuracy as shown in the figure 9 and figure 10. Also the time taken by ABC-SVM is very less compared to GA-SVM to generate optimized values of SVM parameters.

VI. CONCLUSION

This research introduces a novel technique for pain detection. An unsupervised moment and histogram analysis are integrated in the compact altered field using the contourlet transform. The feature extraction using Gabor and contourlet filters are very fast, correct and extremely towering in terminology of appearance detection. The features extracted from the fusion of CT-GT used for the classification. The proposed GA-SVM and ABC-SVM models, with these combined features, can be automated to determine the optimal values of SVM parameters and exhibits increased classification accuracy in specified datasets. The proposed ABC-based approach has good classification accuracy compared to the Genetic algorithm. This implementation depicts experimental results with the different kernels. The result analysis in a comparative framework demonstrates the better functionality of the suggested strategy compared to other existing techniques.

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